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Pathological ultrastructural alterations of myelinated axons in normal appearing white matter in progressive multiple sclerosis



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Abstract

Multiple sclerosis (MS) pathophysiology includes inflammation, demyelination and neurodegeneration, but the exact mechanisms of disease initiation and progression are unknown. A major feature of lesions is lack of myelin, which increases axonal energy demand and requires adaptation in number and size of mitochondria. Outside lesions, subtle and diffuse alterations are observed in normal appearing white matter (NAWM) and normal appearing grey matter (NAGM), including increased oxidative stress, reduced axon density and changes in myelin composition and morphology. On an ultrastructural level, only limited data is available on alterations in myelinated axons. We generated large scale 2D scanning transmission electron microscopy images ('nanotomy') of non-demyelinated brain tissue of control and progressive MS donors, accessible via an open-access online repository. We observed a reduced density of myelinated axons in NAWM, without a decrease in cross-sectional axon area. Small myelinated axons were less frequently and large myelinated axons were more frequently present in NAWM, while the g-ratio was similar. The correlation between axonal mitochondrial radius and g-ratio was lost in NAWM, but not in NAGM. Myelinated axons in control GM and NAGM had a similar q-ratio and radius distribution. We hypothesize that axonal loss in NAWM is likely compensated by swelling of the remaining myelinated axons and subsequent adjustment of myelin thickness to maintain their g-ratio. Failure of axonal mitochondria to adjust their size and fine-tuning of myelin thickness may render NAWM axons and their myelin more susceptible to injury.

Keywords Electron microscopy, g-ratio, Human brain (bank), Mitochondria, Multiple sclerosis, Myelin, Nanotomy, Ultrastructure

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Introduction

Multiple sclerosis (MS) is a chronic neuroinflammatory and neurodegenerative disease of the central nervous system (CNS), in which demyelinated lesions occur in white and grey matter. Although non-demyelinated tissue appears macroscopically normal, it is referred to as normal appearing white (NAWM) or grey matter (NAGM), and neuroimaging, histopathological and biochemical studies showed that NAM differs from white (CWM) and grey matter (CGM) of control subjects. For example, NAWM and NAGM of relapsing remitting (RRMS) and progressive MS (SPMS/PPMS) contain magnetic resonance abnormalities that are more pronounced in NAWM [1-3]. In addition, the density of myelinated axons in NAGM [4] and NAWM [5] is reduced. Microglia are in a more activated state [6-10] and an increase in reactive oxygen species (ROS) causes oxidative damage in NAM [11]. Alterations in extracellular matrix components in NAWM contribute to a nonpermissive environment for axon regrowth and remyelination [12]. The widespread pathological changes in non-lesioned tissue are more prominent in late progressive MS, and in NAWM often correlate with lesion load and/or magnetisation transfer imaging (MTR) abnormalities [3, 13-15], indicating a potential secondary response to neurodegeneration.

Myelin structure and composition in NAWM are also abnormal. The nodes of Ranvier are disrupted, as evidenced by an increased overlap of the juxtaparanodes and paranodes [16-19]. In addition, MS myelin is biochemically different from myelin of control donors. Bulk analysis of myelin showed a shift in the lipid composition of NAWM to a higher phospholipid and lower sphingolipid content [20] as well as indication of changed lipid packing [21] and posttranslational alterations, namely citrullination and acylation, of myelin proteins like myelin basic protein [22, 23]. Next to these global changes in myelin composition, local blisterlike swellings are formed by myelin detachment from axons [19, 24] and activated microglia clusters spatially accumulate in NAWM [25, 26], which may reflect early pathology of MS. Indeed, NAWM abnormalities in early RRMS display lesion-independent pathology

[27], and MRI-based findings confirm that alterations in NAWM likely occur before lesion formation [15, 28, 29], which may relate to oligodendrocyte pathology or damage to the neuroaxonal unit.

An important structural property reflecting axonal function and integrity is the ratio of the inner and outer diameter of the myelin sheath ('g-ratio'), which needs to be optimal for effective speed of impulse conduction [30, 31]. To comply with the altered energy demands upon demyelination and at a (sub)optimal g-ratio, axons adapt by adjusting the number and size of mitochondria and increase the speed of their transport [32, 33]. Remyelinated axons, hallmarked by thinner myelin sheaths, and therefore a higher g-ratio, have an increased mitochondrial content compared to myelinated axons [34]. Myelinated axons in NAWM have a lower mitochondrial content than myelinated axons in CWM [34]. In contrast, the number of mitochondria in myelinated axons is increased in optic nerve NAWM [18].

Identifying (sub)cellular and ultrastructural morphological changes of individual myelinated axons may help to understand pathological mechanisms in MS. Electron microscopy (EM) data on human MS brain tissue is very limited, and largely depends on studies from the 1960's and 70's that merely focused on lesions in small selected areas [35, 36]. The last decade higher throughput EM techniques provide more quantitative ultrastructural information of relatively large tissue areas (mm² range) [37, 38]. Indeed, g-ratio analysis and the reported morphological changes in myelinated axons in NAM are just starting to be analysed at nanoscale resolution [18]. To obtain further insight into myelinated axonal pathology in NAM, we (1) determined ultrastructural features of myelinated axons and their mitochondria in CGM, NAGM, CWM and NAWM and (2) generated an open access database to vist and reuse the digitalized donor tissue in a Google Earth-like manner.

Materials and methods

Study design

Fresh post-mortem human brain tissue of progressive MS (NAWM, NAGM) and control donors (CWM, CGM) were processed for large scale STEM (nanotomy) and an EM database was created. The datasets were analysed for ultrastructural alterations of crosssectional myelinated axons, axonal mitochondria, dendrites and dendritic mitochondria. For white matter, ultrastructural characteristics of 200 myelinated axons and their mitochondria were analysed per dataset, including density and total axon area of the myelinated axons. For grey matter, 100–200 myelinated axons and 200 dendrites and their mitochondria were analysed per dataset.

Donors and sample collection

Fresh post-mortem white and grey matter brain tissue samples from donors with progressive MS and donors without neurological disease were obtained from the Netherlands Brain Bank (Table 1). Tissues were transported in cold HBSS with phenol red (Gibco, #14170-088) supplemented with 15 mM HEPES (Gibco, #15630-056) and 0.6% glucose (Sigma, #G8769). 4 control donors and 7 donors with progressive MS (mean disease duration 23 ± 4.2 years) were included in this study (Table 1). NAGM 7 was excluded because myelinated axons were absent. The male/female ratio for control donors was 3:1, and for donors with MS 4:3 for NAWM and 2:1 for NAGM. The median age of death of the control donors $(77 \pm 4.5 \text{ years})$ was significantly higher than the MS donors $(61 \pm 8.0$ years for NAWM and 62 ± 8.7 years for NAGM). Post-mortem delay was comparable between control donors and donors with progressive MS. Informed consent was obtained by the Netherlands Brain Bank and the procedure approved by the Ethical Committee (Amsterdam UMC, the Netherlands).

Electron microscopy

Upon arrival, fresh white and grey matter brain tissue samples were cut into $\sim 1-3$ m³ pieces and fixated in cold 2% paraformaldehyde (PFA; Merck, #104005)-2% glutaraldehyde (GA; Polysciences, #01909) in 0.1M cacodylate buffer pH 7.4 (Sigma-Aldrich, #20840) and stored at 4 °C until further processing. Alternatively, 2% PFA-0.5% GA was used (dataset CM 1). After primary fixative (2-35 days, median of 6 days) samples were washed three times for 5 min with 0.1M cacodylate buffer and post-fixed in 1% osmium tetroxide (Electron Microscopy Sciences #19114) -1.5% potassium ferrocyanide (Merck, #P9387) in 0.1M cacodylate buffer for 2 h at 4 °C. After post-fixation, samples were washed four times for 5 min with MilliQ followed by dehydration and embedding in epoxy resin (glycid ether 100; SERVA, #21045, 2-Dodecenylsuccinic acid anhydride; SERVA, #20755, Methylnadic anhydride; SERVA; #29452, DMP-30; Polysciences, #00553). Semi-thin (~1 μ m) sections were stained with toluidine blue to check if samples were homogenous in morphology. Samples were then trimmed to fit the grids, and ultrathin (~80 nm) sections were cut on an ultramicrotome with a diamond knife (Diatome, ultra 45°) and carefully positioned on formvar-coated copper L2×1 grids (Agar Scientific, #AGG2500C). Finally, sections were contrasted with 4% neodymium (III) acetate

Donor ^a	Neur. ^b diagnosis	Cause of death	Sex	M:F	Age	$med \pm SD^d$	PMD (h:min) ^c	$med\pmSD$	Disease duration (years)	$med\pmSD$
CM ^e 1	_	Esophageal cancer	М	3:1	82	76±4.0*	06:30	06:57±1:51	_	
CM 2	-	Metastatic prostate cancer	М		77		07:25		-	
CM 3	_	Collapse, followed by asystole. probably cardiac death	Μ		73		10:15		_	
CM 4	-	Euthanasia	F		74		06:10		-	
NAM ^f 1▲	PPMS	Respiratory insufficiency due to MS, assumed pneu- monia	Μ	WM 4:3 GM 2:1	56	WM 61±8.0* GM 62±8.7*	06:15	WM 08:04±1:24 GM 08:01±1:32	20	WM 23±4.2 GM 24±4.4
NAM 2	SPMS	Euthanasia	F		66		09:30		25	
NAM 3	SPMS	Renal failure	М		53		06:25		24	
NAM 4	PMS	Sepsis	F		65		09:30		33	
NAM 5	SPMS	Euthanasia	М		58		08:59		23	
NAM 6🔺	SPMS	Euthanasia	М		77		07:04		23	
NAWM ^g 7•	SPMS	Urosepsis, hydronephrosis	F		61		08:04		22	

 Table 1
 Donor information of white and grey matter human brain tissue samples

*Median age of death was significantly higher in CM than in NAM (p < 0.05, Student's t test)

^a Color icons are consistently used throughout the manuscript

^b Neurological diagnosis

^c Post-mortem delay from the Netherlands Brain Bank, excluding the transport time on ice (approx. 2 h) to the lab

 d Median \pm standard deviation

e Control matter

^f Normal appearing (white and grey) matter

^g normal appearing white matter

(Sigma-Aldrich, #325805) in MilliQ [39], washed five times with MilliQ and carefully dried and stored in a gridbox.

EM acquisition and image processing

Image data were acquired on a Supra 55 scanning EM (SEM; Zeiss) using a scanning transmission EM (STEM) detector at 28 kV/25 kV with 2.5 nm pixel size with an external scan generator ATLAS 5 (Fibics) as previously described [40]. One dataset was made of 47 ± 21 tiles, one tile sized 16 k×16 k pixels. The median dataset area is 70 k µm². After image tile stitching, sample datasets were exported as html files and uploaded to the website https://www.nanotomy.org. Each dataset can be accessed at full resolution.

Image analysis

Individual myelinated axons

From each dataset, 20 areas of $30 \times 30 \ \mu\text{m}$ were exported from the html file at a resolution ~ 20 nm/pixel. The variation in shape and the frequency of touching axons in human brain tissue precluded the use of most publicly available (semi)automated tools, and preferred the use of the Gratio plugin tool from Fiji (http://gratio.efil.de/) [41, 42]. From each area, the tool randomly selected 10 cross-sectional myelinated axons per area from which the g-ratio was determined (n = 200 per donor for white)matter, n = 100-200 per donor for grey matter). The analysis was performed by selecting the inner and the outer perimeter of the myelin sheath. The enclosed areas were used to automatically determine the g-ratio. The axon radius and myelin thickness were calculated from enclosed areas. Notably, the Gratio plugin tool does not take into account the inner tongue area, potentially leading to an overestimation of the axon radius. The compactness of the myelin sheath of the 200 measured axons was scored with a system ranging from 1 to 5, in which score 1 represents almost fully compact myelin and score 5 contains splits of the myelin layers along >70% of the cross-sectional axon area. The presence of mitochondria in the myelinated axons was scored, and the crosssectional mitochondrial size (area, radius, perimeter) and shape (circularity) were determined using Fiji.

Myelinated axon density and total myelinated axon area

From each white matter dataset, 25 areas of $20 \times 20 \ \mu m$ were exported from the html file at a resolution around 20 nm/pixel. Areas without capillaries were selected, to prevent bias in the measurements. The number of myelinated axons and total axonal area, measured as the area enclosed by myelin, of each image were determined using Fiji.

Individual dendrites

From each grey matter dataset, the same areas used for analysis of individual myelinated axons were analysed for dendrites and their mitochondria. From each area, the dendritic area of 10 randomly selected dendrites was determined (n=200 per donor) using the Gratio plugin tool from Fiji. The presence of mitochondria in the dendrites was scored, and the cross-sectional mitochondrial size (area, radius, perimeter) and shape (circularity) were determined using Fiji.

Statistical analysis

Statistical analysis was performed using R (version 4.1.0, Integrated Development for R. RStudio, Inc., Boston, MA. URL http://www.rstudio.com/). A total of 2200 datapoints were available for statistical analysis of individual myelinated white matter axons (11 donors×200 axons) and dendrites (11 donors × 200 axons). For the myelinated grey matter axons, 1501 datapoints were available (10 donors×100-200 axons). For statistical analysis of individual mitochondria in myelinated axons, the number of available datapoints was; 143 of CWM (4 donors×21-49 mitochondria), 92 of CGM (4 donors $\times 10-40$ mitochondria), 101 of NAGM (6 donors×6-31 mitochondria) and 269 of NAWM (7 donors \times 27–69 mitochondria). For dendritic mitochondria 289 datapoints were available of CGM (4 donors×54-101 mitochondria) and 333 of NAGM (6 donors×44-72 mitochondria). For the axon density and total axon area, 275 datapoints were available (11 donors \times 25 areas). Linear mixed-effect models were used in analysis to account for repeated measures. The nlme package in R was implemented with diagnosis as fixed variable and "donor ID" as a random factor. Including age and/or post-mortem delay (PMD) did not lead to a better model fit. For the comparisons in the percentage of axons/dendrites with mitochondria, the student's t test was used to compare the means (calculated by taking the mean per donor). This test requires that samples are independent, of equal variance and normally distributed. Therefore, the Shapiro-Wilk test was used to confirm these assumptions prior to performing a Student's t test. For the comparisons between control and MS donors, a Student's t test was performed and for comparisons between control grey and white matter, a paired Student's t test was performed. To test whether a linear correlation exists between the mitochondrial radius and the g-ratio, the Pearson correlation coefficient was used. Given the overrepresentation of male donors in our dataset, statistical difference for male donors only was analysed and indicated when significance deviate from the analysis of both sexes. For all statistical analyses p values < 0.05 were considered significant.

Results

Myelinated axons in CGM are smaller and have a higher g-ratio than myelinated axons in CWM

Myelinated axons are more extensively studied in myelinrich white matter than in myelin-poor grey matter tissue. Therefore, we first compared ultrastructural features of myelinated axons and their mitochondria in grey and white matter brain tissue of control donors (Fig. 1A). To this end, CGM and CWM from 4 non-demented control donors were analysed, in which the median dataset area was 70 k µm² (Table 1). As expected, CGM contained less myelinated axons and more neuronal cell bodies and dendrites, while CWM contained mostly myelinated axons (Fig. 1B). As the g-ratio is an important structural trait that affects nerve impulse conduction, we next determined per donor the g-ratio of 200 myelinated axons from CWM and 150-200 myelinated axons from CGM. The g-ratio of myelinated axons in CWM was significantly lower than in CGM (CWM: 0.75 ± 0.015 , CGM: 0.78 ± 0.022 , p < 0.001) (Fig. 1C). In CGM, the measured radius of axons ranged from 0.11 to 1.7 µm, and in CWM from 0.15 to 4.2 µm. Furthermore,

⁽See figure on next page.)

Fig. 1 Myelinated axons in CWM have a lower g-ratio and a higher axon radius than in CGM. **A** Experimental set-up. Post-mortem human brain tissue samples were collected from control donors and donors with progressive MS and processed for large-scale scanning transmission electron microscopy (STEM). Datasets were analysed for ultrastructural features of myelinated axons (a1: g-ratio (r/R), a2: radius (r), a3: density; a4: total area) and their mitochondria (m1: number, m2: area, m3: perimeter, m4: circularity). Each dataset is accessible in full resolution via nanotomy.org. **B** Representative STEM images of post-mortem control grey matter (CGM) and control white matter (CWM) tissue of control donors (paired, from donor CM 1). Top: overview images. Bottom: detailed images from boxed regions in top images. a = myelinated axon, d = dendrite, n = nucleus, bv = blood vessel, m = mitochondria. Scale bar represents 2 μ m (top images) or 0.5 μ m (bottom images). **C**, **D** Violin plots depicting the distribution of g-ratio (**C**) and axon radius (**D**). Datapoints represent mean per donor ($\mathbf{O} =$ female, $\mathbf{A} =$ male, color-coded, see Table 1) and boxplots show the median and inter quartile range (IQR). **E** Histogram with kernel density estimation of the axon radius (r). Number of control (CGM/CWM) donors is 4 (paired). For CGM 100–200 myelinated axons and for CWM 200 myelinated axons per donor were analysed. Statistics were performed using linear mixed model (**C**, **D**), or a paired sample Student's t test (**E**) (*p < 0.05; **p < 0.01; ***p < 0.001)



Fig. 1 (See legend on previous page.)

the radius of myelinated axons was higher in CWM than in CGM (CWM: $0.82 \pm 0.090 \mu$ m, CGM: $0.51 \pm 0.083 \mu$ m, p < 0.001) (Fig. 1D). Frequency density plots of axon radii indicate that CWM contained more large myelinated axons ($0.75-1.75 \mu$ m) and less small myelinated axons ($0.25-0.50 \mu$ m) compared to CGM (Fig. 1E). Hence, myelinated axons in CGM were smaller than myelinated axons in CWM. A higher g-ratio results in increased energy demands of axons to achieve optimal action potential propagation, which can be accomplished by alterations in mitochondria number and/or morphology [43]. Therefore, we next determined ultrastructural features of mitochondria in myelinated axons in CGM and CWM.

Axonal mitochondrial radius in myelinated axons correlates with g-ratio in control matter

To determine whether the higher g-ratio of myelinated axons in CGM may be compensated by alterations in their mitochondria, we determined the number, size and shape of mitochondria present in the myelinated axons analysed in Fig. 1 (Figs. 1A, 2A). The percentage of cross-sectional myelinated axons with mitochondria did not differ between CGM and CWM (Fig. 2B). The cross-sectional area of mitochondria that are present in myelinated CWM axons was smaller compared to the mitochondrial area in myelinated CGM axons, (CWM: $0.21 \pm 0.049 \ \mu\text{m}^2$, CGM: $0.28 \pm 0.058 \ \mu\text{m}^2$, p = < 0.001) (Fig. 2C). The perimeter of mitochondria in myelinated



Fig. 2 Mitochondrial size in myelinated axons correlates with g-ratio in control brain tissue. **A** Cross-sectional image of a myelinated axon with a mitochondrion (m) in post-mortem brain tissue of control donors. Scale bar represents 0.2 μ m. **B** Mean percentage myelinated axons with mitochondria in post-mortem control grey matter (CGM) and control white matter (CWM) tissue of control donors. **C**–**E** Analysis of cross-sectional axonal mitochondrial area (**C**), perimeter (**D**), and circularity (**E**). Icons indicate measured mitochondrial characteristic (red), violin plots depict the data distribution of all measurements, datapoints represent mean per donor (**O** = female, **A** = male, color-coded, see Table 1), and boxplots show the median and inter quartile range (IQR). **F** Scatter plot showing the correlation between mitochondria radius and g-ratio. The size of the datapoints indicates axon radius in μ m. The number of control (CGM/CWM) donors is 4 (paired) and 10–49 mitochondria per donor were analysed (dependent on the number of mitochondria in the 100–200 myelinated axons that were measured in Fig. 1). Statistics were performed using a paired Student's *t* test (**B**), linear mixed model (**C**–**E**), or a Pearson's r test (**F**) (***p < 0.001)

CGM axons was significantly larger than in CWM (CGM: $1.9\pm0.22 \ \mu$ m, CWM: $1.7\pm0.16 \ \mu$ m, p < 0.001) (Fig. 2D). Cross-sectional mitochondria were similar in shape, as indicated by mitochondrial circularity (Fig. 2E). Overall, when the myelinated axons of CWM and CGM were combined, we observed a correlation between the mitochondrial radius and g-ratio (Fig. 2F), indicating homeostatic conditions [43]. To determine potential NAM ultrastructural abnormalities in myelinated axons and their mitochondria, we first compared CGM with NAGM.

Myelinated axons in CGM and NAGM have a similar g-ratio and axon size distribution

To establish whether ultrastructural pathological differences existed in myelinated axons in NAGM, we compared CGM from 4 non-demented control donors with NAGM of 6 donors with progressive MS (Table 1, Figs. 1A, 3A, 100-200 myelinated axons per donor). The onset of MS lesion formation is characterized by myelin decompaction and breakdown. Therefore, we first assessed myelin structure in CGM and NAGM using a scoring system based on the extent of (de)compaction (Additional file 1: Fig. S1A). The proportions of myelin compaction scores in NAGM were similar to the proportions in CGM (Additional file 1: Fig. S1B), indicating that there were no signs of substantial (early) demyelination in the analysed areas. Myelinated axons in CGM and NAGM had a similar g-ratio (Fig. 3B). The logarithmic regression curves in the g-ratio versus axon scatter plots did not completely overlay for larger axons (Fig. 3C). Larger myelinated axons in NAGM tended to have a higher g-ratio, which may point to remyelination, consistent with a previous study [44]. Axon radii analysis indicated no major difference between the distribution in CGM and NAGM (Fig. 3D). Hence, myelinated axons in CGM and NAGM have a similar g-ratio and axon radius distribution.

Axonal mitochondrial radius correlates with g-ratio in NAGM

To determine whether potential alterations in energy supply by mitochondria exist, we determined whether mitochondria in myelinated axons in NAGM were changed. From the same myelinated axons that were measured in Fig. 3, we counted the number of myelinated axons with at least one mitochondrion and determined the crosssectional mitochondrial area, perimeter and circularity (Fig. 4). The percentage of cross-sectional myelinated axons with mitochondria ranged from 5 to 31% and did not differ between CGM and NAGM (Fig. 4A). Axonal mitochondria in NAGM have a similar cross-sectional area and perimeter, (Fig. 4B, C), unless if for perimeter only male donors were compared (p = 0.039). The mitochondrial circularity was similar between CGM and NAGM (Fig. 4D). Furthermore, the mitochondrial radius and g-ratio correlated in NAGM (Fig. 4E), indicating homeostatic conditions. This correlation was not statistically significant within the p < 0.05 limit in CGM.

In addition to the analysis of myelinated axons and axonal mitochondria, we analysed the ultrastructural characteristics of 200 dendrites and their mitochondria in the same CGM and NAGM areas (Additional file 2: Fig. S2A). The total cross-sectional dendritic area was similar in CGM and NAGM (Additional file 2: Fig. S2B). Furthermore, the percentage of cross-sectional dendrites that contain mitochondria was similar in NAGM and CGM (Additional file 2: Fig. S2C, NAGM: 28±5.4%, CGM: $36 \pm 11\%$). Notably, the percentage of cross-sectional dendrites with mitochondria was higher than in myelinated axons (Additional file 2: Fig. S2C versus 4A, GM dendrites: $31 \pm 8.7\%$, GM axons: $13 \pm 9.0\%$, p < 0.001). The cross-sectional dendritic mitochondrial area, perimeter and circularity were similar in CGM and NAGM (Additional file 2: Fig. S2D-F). Thus, we observed no significant differences in cross-sectional axonal and dendritic mitochondria number, size and shape between CGM and NAGM.

NAWM contains fewer myelinated axons that cover a similar cross-sectional axonal area as in CWM, while g-ratio is maintained

To identify potential ultrastructural alterations in NAWM of progressive MS donors, we compared CWM from 4 non-demented control donors with NAWM from 7 donors with progressive MS (Table 1, Figs. 1A, 5A, 200 myelinated axons per donor). In NAWM there were no signs of (early) demyelination, as evidenced by similar proportions in myelin compaction scores in CWM and NAWM (Additional file 1: Fig. S1A, C). The number of myelinated axons per 400 μ m² was 1.5fold lower in NAWM compared to CWM (Fig. 5A, B, NAWM: 59±8.4, CWM: 86±6.9, *p*<0.001). Strikingly, myelinated axons in CWM and NAWM covered a similar cross-sectional total axon area (Fig. 5C). A rightward shift of the peak in NAWM compared to CWM, indicates enlarged myelinated axons in NAWM. More specifically, NAWM significantly contained less myelinated axons with an axon radius < 0.25 μ m (Fig. 5D, p = 0.010) and more myelinated axons with an axon radius between 2.25 and 2.50 μ m (Fig. 5D, *p*=0.039) and tended to have more myelinated axons with an axon radius between 1.25 and 1.50 μ m (Fig. 5D, p = 0.056). Intriguingly, in spite of the enlarged axons, no differences in the g-ratio (Fig. 5E) and scatter plots of g-ratio versus axon radius (Fig. 5F)



Fig. 3 Myelinated axons in CGM and NAGM have a similar g-ratio and axon size distribution. **A** Representative scanning electron microscopic images (STEM) images of post-mortem control grey matter (CGM) of control donors (from donor CM 2) and normal appearing grey matter (NAGM) of donors with progressive MS (from donor NAM 6). Top: overview images. Bottom: detailed images from boxed regions in top images. Scale bars represent 2 μ m (top images) or 0.5 μ m (bottom images). **B** Violin plots depict the distribution of g-ratio (r/R). Datapoints represent mean per donor (\bigcirc = female (SPMS), \triangle = male (SPMS), \triangle = male (PPMS), color-coded, see Table 1) and boxplots show the median and inter quartile range (IQR). **C** Scatter plot showing the g-ratio versus axon radius (log-linear fit). **D** Histogram with kernel density estimation of the axon radius (r). Number of control donors (CWM) is 4, number of donors with progressive MS (NAWM) is 6, and 100–200 myelinated axons per donor were analysed. Statistics were performed using a linear mixed model (**B**) or unpaired Student's t test (**D**)

between CWM and NAWM were noticed. Thus, NAWM contains fewer but larger myelinated axons covering a

similar cross-sectional myelinated axon area as in CWM, while their g-ratio is maintained.



Fig. 4 Axonal mitochondrial size correlates with g-ratio in NAGM. **A** Mean percentage myelinated axons with mitochondria in post-mortem control grey matter (CGM) of control donors and normal appearing grey matter (NAGM) tissue of donors with progressive MS. **B**–**D** Analysis of cross-sectional axonal mitochondrial area (**B**), perimeter (**C**), and circularity (**D**). Icons indicate measured mitochondrial characteristics (red), violin plots depict the data distribution of all measurements, datapoints represent mean per donor (\bullet = female (SPMS), \blacktriangle = male (SPMS), \bigtriangleup = male (PPMS), color-coded, see Table 1), and boxplots show the median and inter quartile range (IQR). **E** Scatter plot showing the correlation between mitochondria radius and g-ratio. The size of the datapoints indicates the axon radius in µm. Number of control donors (CGM) is 4, number of donors with progressive MS (NAGM) is 6, and 6–40 mitochondria per donor (dependent on the number of mitochondria in the 100–200 axons that were measured in Fig. 3) were analysed. Statistics were performed using an unpaired Student's *t* test (**A**), linear mixed model (**B**–**D**), or a Pearson's r test (**E**)

Axonal mitochondrial radius does not correlate with g-ratio in NAWM

To reveal whether the observed pathology of myelinated axons in NAWM affect mitochondria, we next determined mitochondria number and morphology. We counted the number of myelinated axons with at least one mitochondrion and determined the mitochondrial area, perimeter and circularity in the white matter from the same myelinated axons that were analysed in Fig. 5. From the 200 cross-sectional myelinated axons in NAWM that were analysed per donor, 11–35% contained mitochondria, which was not significantly different from CWM (Fig. 6A). The cross-sectional area, perimeter and circularity of mitochondria present in cross-sectional

(See figure on next page.)

Fig. 5 Reduced myelinated axon density in NAWM, while total myelinated axon area and g-ratio are unaffected. **A** Representative scanning transmission electron microscopic images (STEM) images of post-mortem control white matter (CGM) of control donors (from donor CM 1) normal appearing white matter (NAWM) of donors with progressive MS (from donor NAM 6). Top: overview images. Bottom: detailed images from boxed regions in top images. n = nucleus, bv = blood vessel, m = mitochondria. Scale bars represent 5 μ m (top images) or 0.5 μ m (bottom images). **B**, **C** Violin plots depict the number of myelinated axons (**B**) and their total area (**C**, red) in an area of 20 × 20 μ m. **D** Histogram with kernel density estimation of the axon radius (r). **E** Violin plot depicts the distribution of g-ratio (r/R). Datapoints represent mean per donor (**B**, **C**, **E** • = female (SPMS), Δ = male (SPMS), Δ = male (PPMS), color-coded, see Table 1) and boxplots show the median and inter quartile range (IQR). **F** Scatter plot showing the g-ratio versus axon radius (log-linear fit). Number of control donors (CWM) is 4, number of donors with progressive MS (NAWM) is 7, 200 myelinated axons per donor (**D**–**F**), and 25 areas of 20 × 20 μ m (**B**, **C**) were analysed. Statistics were performed using an unpaired Student's *t* test (**D**), or a linear mixed model (**B**, **C**, **E**) (*p < 0.05; **p < 0.01;



Fig. 5 (See legend on previous page.)



Fig. 6 Axonal mitochondrial size does not correlate with g-ratio in NAWM. **A** Mean percentage myelinated axons with mitochondria in post-mortem control white matter (CWM) of control donors and normal appearing white matter (NAWM) tissue of progressive MS donors. **B**–**D** Analysis of cross-sectional axonal mitochondrial area (**B**), perimeter (**C**), and circularity (**D**). Icons indicate measured mitochondrial characteristics (red), violin plots depict the data distribution of all measurements, datapoints represent the mean per donor (\bigcirc = female (SPMS), \triangle = male (SPMS), \triangle = male (PPMS), color-coded, see Table 1) and boxplots show the median and inter quartile range (IQR). **E** Scatter plot showing the correlation between mitochondria radius and g-ratio. The size of the datapoints indicates the axon radius in µm. Number of control donors (CWM) is 4, number of donors with progressive MS (NAWM) is 7, and 21–69 mitochondria per donor (dependent on the number of mitochondria in the 200 myelinated axons that were measured in Fig. 5) were analysed. Statistics were performed using an unpaired Student's *t* test (**A**), linear mixed model (**B**–**D**), or a Pearson's r test (**E**)

myelinated axons in CWM and NAWM were also similar (Fig. 6B–D). Interestingly, we observed a correlation between the mitochondrial radius and the g-ratio in CWM, while this correlation was absent in NAWM (Fig. 6E). This indicates that axons in NAWM fail to adapt their mitochondrial radius to correct for a suboptimal g-ratio.

Discussion

Conventional techniques, like MRI and immunohistochemistry, revealed signs of both early and late axonal pathology in non-demyelinated tissue of donors with progressive MS. Here, using large scale electron microscopical analysis (nanotomy) of post-mortem human brain tissue, we show that less myelinated axons in nonlesioned white matter of donors with progressive MS cover the same myelinated axon area as white matter of control donors. To compensate for the reduced density, myelinated axons in NAWM are enlarged, while retaining a similar g-ratio as myelinated axons in CWM (Fig. 7). In addition, the lack of correlation between axonal mitochondrial radius and g-ratio in NAWM indicate a disturbance in homeostasis [43] and the inability of mitochondria to adjust to a suboptimal g-ratio. In contrast to NAWM, the ultrastructural characteristics of myelinated axons and their mitochondria in the NAGM were similar compared to CGM. Hence, these ultrastructural changes in myelinated axons point to pathological alterations in (progressive) MS that may make NAWM myelin more susceptible to injury [29]. Our generated datasets are transferred into an open access database, and the systemic inclusion of higher numbers of donors that can be studied, like has been done before with nPOD [37], will not only allow to



Fig. 7 Hypothetical model explaining myelinated axon pathology in normal appearing white matter (NAWM) based on the observed ultrastructural abnormalities in myelinated axons. We argue that a loss of small calibre myelinated axons in NAWM of persons with progressive MS results in a lower myelinated axon density. To compensate for the loss of myelinated axons, remaining axons swell (pink arrow) to increase their size to cover a similar axon area. The swelled axons adjust their myelin thickness (green), explaining the unaltered g-ratio, to preserve axonal shape and limit further swelling

increase group size, but also makes the data directly available to others and reuse for future additional analysis, which may focus on other ultrastructural features.

Currently, information on spatial variation, including in grey versus white matter, of the g-ratio of individual axons in human brain tissue is limited. We provide systematic information regarding the g-ratio of individual myelinated axons and their mitochondria in nonlesioned grey and white matter in control and progressive MS donors. In the CNS, a g-ratio of approx. 0.77 is considered to be theoretically optimal [45]. Our analysis of individual myelinated axons in relatively large post-mortem brain tissue samples provided a g-ratio of 0.75 in CWM and 0.78 in CGM. Additionally, myelinated axons in CWM were larger than myelinated axons in CGM. MRI-based studies in control subjects report a different g-ratio. An aggregated g-ratio of 0.7 in CWM was reported using magnetization transfer with neurite orientation dispersion and density imaging (NODDI) [46] and magnetization transfer with single-shell diffusion MRI [47]. While a g-ratio of 0.71–0.85 was reported in CWM using multi-echo gradient echo myelin water imaging and NODDI [48]. Our reported g-ratio in NAWM (0.76) is higher than previously reported aggregated g-ratio's in NAWM, i.e., 0.67 using high-gradient diffusion MRI and macromolecular tissue volume imaging [49] and 0.57 using magnetization transfer saturation and NODDI [50]. Notably, the aggregated g-ratio value obtained with MRI-based techniques depends on the used method and calculation model [51] and are more sensitive to changes or differences in large diameter axons [52]. Our analysis further revealed that the g-ratio of individually analysed myelinated axons in non-lesioned grey and white matter was similar between control donors and donors with progressive MS. This is in contrast with a recent study in post-mortem optic nerve tissue in which the g-ratio of myelinated axons in CWM was higher (0.53) than in NAWM (0.50) [18]. In addition, myelin in optic nerve NAWM was less compact and the number of mitochondria in myelinated axons was higher, while axon density and diameter were similar between optic nerve NAWM and CWM [18]. Most importantly, the authors suggest that the ultrastructural abnormalities correlated with inflammation in adjacent tissue. In contrast, we find that myelinated axons in NAWM and CWM had similar proportions of the myelin compaction score, and that the analysed areas had a similar number of non-endothelial nuclei that were evenly distributed (CWM 57±15 and NAWM 42 ± 18 per median dataset area of 70 k μ m², p=0.176). The lack of obvious signs of increased cell density by e.g., glial cell proliferation or infiltration, and decompaction, does however not exclude that the glial cells present in our dataset exhibit inflammatory alterations and/or may take up more space between myelinated axons.

The observed lower cross-sectional myelinated axon density in NAWM is consistent with (indirect) previous findings [5, 53, 54] and is likely a consequence of loss of small calibre myelinated axons, although regional differences in axon size in white matter tracts cannot be excluded. Based on the shift in frequency distribution towards larger calibre axons and a similar total axon area compared to CWM, we argue that the loss of small calibre axons is compensated by swelling of remaining myelinated axons. This is consistent with the previously reported focal swellings of axons without signs of demyelination in NAWM [19, 55]. Pathological features of swelled axons are accumulation of intra-axonal

organelles and/or an increase in neurofilament spacing [55–58], most prominent in small calibre axons. The frequency of these features is most reliably analysed in 3D and/or longitudinal axonal scans. Equally reasonable, these features may resolve in NAWM as swelled myelinated axons may recover by adjusting their myelin thickness, explaining the unaltered g-ratio. This may overcome disrupted axonal conduction and preserve axonal shape by limiting further swelling as recently proposed [56]. This implies that the thickness of pre-existing myelin is not static and that mature oligodendrocytes are able to re-instate myelin membrane expansion. In control CNS, myelin sheaths continuously undergo dynamic remodelling, which is guided by neuronal activity known as OPC-based adaptive myelination [57]. Accordingly, it is tempting to suggest that the adjustment of myelin thickness in NAWM is a response of mature oligodendrocytes to altered activity of swelled axons to re-establish myelin biogenesis, i.e., oligodendrocyte-based adaptive myelination. In adult mice, newly made myelin components for e.g., myelin turnover and maintenance, are integrated at the paranodal and juxtaparanodal regions at the inner tongue [58]. Therefore, adaptive myelination by mature oligodendrocytes initiated by axonal swelling may contribute the elongation of (juxta)paranodal lengths observed in NAWM [16–19]. Furthermore, as the adjustment of myelin sheath thickness requires biosynthesis of myelin constituents, we argue that this re-instated myelination by mature oligodendrocytes causes changes in the myelin composition compared to myelin that is formed during development. This hypothesis is strengthened by reported subtle biochemical differences between NAWM and CWM myelin, and the notion that NAWM myelin is developmentally immature [20-23]. Further research is necessary to determine whether axonal swelling and subsequent adjustment of the myelin thickness indeed induces compositional changes in MS NAWM myelin.

An important remaining question is why axon density is decreased in NAWM. In murine experimental autoimmune encephalomyelitis (EAE), an experimental model mimicking inflammatory aspects of MS, axon density is also decreased in non-demyelinated white matter areas of the spinal cord, along with ongoing demyelination, axolysis and mitochondrial swelling [59]. Of note, in this EAE study, the analysed nondemyelinated areas were perilesional and may therefore harbor more extensive changes compared to white matter further away from the demyelinated areas. In acute spinal EAE lesions in mice, axonal swellings are an early ultrastructural sign of damage that precede demyelination [55]. Interestingly, some of these swollen axons recovered spontaneously, indicating that axonal swelling can be reversible. Therefore, it is tempting to suggest that by adjusting myelin thickness the myelinated axons may recover from axonal swelling. The potential consequence of axonal swellings is a decrease in conduction velocity [60]. Axonal swelling is thought to be triggered by mitochondrial pathology induced by macrophage-derived reactive oxygen and nitrogen species [55]. Although we did not observe ultrastructural differences between mitochondria in NAWM and CWM in our cross-sectional analysis, we did find that the correlation between the cross-sectional mitochondrial radius and g-ratio shown at homeostatic conditions [43], was lost in NAWM of donors with progressive MS. This may point at the inability of mitochondria to adapt to the increased myelin thickness of enlarged axons [43]. Due to the limitations of EM imaging, we can however not exclude axonal mitochondrial swelling in NAWM and/or alterations in number, localisation and proper functioning of axonal mitochondria.

Apart from analysis of end stage post-mortem brain tissue, limitations of our study are that the control donors were older than the MS donors and mainly males. While sex differences in g-ratio occur during adolescence [61], the data on the influence of sex on g-ratio in adults are conflicting. One MRI-based study showed that the whole-brain g-ratio is not influenced by sex [46], while other studies observed a smaller g-ratio, and thus higher myelin content, in whole-brain of females [62]. In our data, no clear segregation based on sex within the group of MS donors for most tested parameters was detected. In contrast, axon density decreases and g-ratio increases with age [46, 62, 63]. Thus, estimation of myelin volume fraction and axonal volume fraction of MRI images indicate that aggregate g-ratio values increase from middle age in most regions examined. In mouse optic nerve, using three-dimensional EM, ageing axons are larger and have thicker myelin and larger mitochondria [64]. Hence, the age difference between our control and MS donors might underrepresent the lower axon density and larger calibre axons observed in NAWM compared to CWM.

In summary, our findings indicate a loss of small calibre myelinated axons in NAWM and we argue that this is loss is compensated by swelling of remaining axons that adjust their myelin thickness to maintain their g-ratio without adaptation of mitochondria size (Fig. 7). These subtle ultrastructural changes in NAWM point to pathological alterations in progressive MS. As in EAE, axonal swelling might be spontaneously reversible and/or an ultrastructural sign of damage that precedes demyelination. More insight in potential (biochemical) abnormalities of myelin on (recovered) swelled axons may uncover subtle disruption in myelin structure that for example contributes to the increased risk of MS myelin to (ongoing) degeneration and/or elicit (secondary) pathological inflammation. Furthermore, identification of (axonal) signals that re-instate either myelin biogenesis or the response of mitochondria to the adapted g-ratio may lead to novel and more effective therapeutic strategies to halt white matter lesion formation in MS.

Abbreviations

CGM	Control grey matter
CM	Control matter
CNS	Central nervous system
CWM	Control white matter
EAE	Experimental autoimmune encephalomyelitis
EM	Electron microscopy
MRI	Magnetic resonance imaging
MS	Multiple sclerosis
MTR	Magnetisation transfer imaging
NAGM	Normal appearing grey matter
NAM	Normal appearing matter
NAWM	Normal appearing white matter
NODDI	Neurite orientation dispersion and density imaging
nPOD	Network for pancreatic organ donors with diabetes
OPC	Oligodendrocyte progenitor cell
PPMS	Primary progressive multiple sclerosis
ROS	Reactive oxygen species
RRMS	Relapsing remitting multiple sclerosis
SPMS	Secondary progressive multiple sclerosis
STEM	Scanning transmission electron microscopy

Supplementary Information

The online version contains supplementary material available at https://doi. org/10.1186/s40478-023-01598-7.

Additional file 1: Fig. S1. CM and NAM have similar proportions of myelin compaction scores. A Schematic and representative scanning transmission electron microscopic image of cross-sectional myelinated axons with myelin compaction scores ranging from 1–5. The percentage indicates the estimated compact myelin area. Scale bars represent 0.5 µm. B Average proportions of myelin compaction scores in control grey matter (CGM) of control donors and normal appearing grey matter (NAGM) of donors with progressive MS. C Average proportions of myelin compaction scores in control white matter (CWM) of control donors and normal appearing white matter (NAWM) of donors with progressive MS. Statistics were performed using a general linear multivariate model test (SPSS 28, not significant).

Additional file 2: Fig. S2. Dendritic mitochondria in CGM and NAGM are similar. A Representative scanning transmission electron microscopic cross-sectional image of a dendrite with a mitochondrion in post-mortem grey matter brain tissue. Scale bar represents 0.25 µm. B Mean percentage of dendrites with mitochondria in post-mortem control grey matter (CGM) of control donors and normal appearing grey matter (NAGM) tissue of donors with progressive MS. C-E Analysis of cross-sectional dendritic mitochondrial area, perimeter, and circularity. Icons indicate measured mitochondrial characteristics, violin plots depict the data distribution of all measurements, data points represent mean per donor, \blacktriangle = male, Δ = male, color-coded, see Table 1), and boxplots show the median and inter quartile range. Number of control donors is 4 and number of donors with progressive MS is 6. 200 dendrites per donor were analysed of which the number of dendritic mitochondria ranged from 44-101. Statistics were performed using an unpaired Student's t test or linear mixed model (not significant).

Acknowledgements

We acknowledge expert technical assistance by Michel Meijer and Anouk Wolters.

Author contributions

WB conceived the study. WO and KK performed the experiments. WO and AJH acquired the data. WO analyzed and visualized the data. WO, BNGG, SMK, BJLE and WB interpreted the data. WO wrote the manuscript. BNGG, SMK, BJLE and WB critically revised the manuscript. BJLE, WB, BNGG and WO obtained funding. All authors read and approved the final version of the manuscript.

Funding

This work was supported by the Dutch MS Research Foundation (Stichting MS Research, 18-733c MS, MSCNN project grant and 18-1001 MS, out-of-the-box, made possible by MoveS), and the Stichting de Cock–Hadders (WO). Part of the work has been performed in the UMCG Microscopy and Imaging Center (UMIC), sponsored by IMDAP: EU-REACT European regional development fund funded as part of the Union's response to the COVID-19 pandemic; ZonMW grant 91111.006 and the Netherlands Electron Microscopy Infrastructure (NEMI; NWO 184.034.014).

Availability of data and materials

The datasets generated and analysed in the current study are available at full resolution at nanotomy.org.

Declarations

Ethics approval and consent to participate

Fresh post-mortem brain tissue samples were obtained from the Netherlands Brain Bank. Informed consent was obtained by the Netherlands Brain Bank and the procedure approved by the Ethical Committee (Amsterdam UMC, The Netherlands).

Consent for publication

Not applicable.

Competing interests

The authors declare that they have no competing interests.

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Received: 17 April 2023 Accepted: 2 June 2023 Published online: 20 June 2023

References

- Miller DH, Thompson AJ, Filippi M (2003) Magnetic resonance studies of abnormalities in the normal appearing white matter and grey matter in multiple sclerosis. J Neurol 250:1407–1419. https://doi.org/10.1007/ S00415-003-0243-9
- Griffin CM, Chard DT, Parker GJM et al (2002) The relationship between lesion and normal appearing brain tissue abnormalities in early relapsing remitting multiple sclerosis. J Neurol 249:193–199. https://doi.org/10. 1007/PL00007864
- Ramió-Torrentà L, Sastre-Garriga J, Ingle GT et al (2006) Abnormalities in normal appearing tissues in early primary progressive multiple sclerosis and their relation to disability: a tissue specific magnetisation transfer study. J Neurol Neurosurg Psychiatry 77:40. https://doi.org/10.1136/JNNP. 2004.052316
- Klaver R, Popescu V, Voorn P et al (2015) Neuronal and axonal loss in normal-appearing gray matter and subpial lesions in multiple sclerosis. J Neuropathol Exp Neurol 74:453–458. https://doi.org/10.1097/NEN.00000 00000000189
- Evangelou N, Esiri MM, Smith S et al (2000) Quantitative pathological evidence for axonal loss in normal appearing white matter in multiple sclerosis. Ann Neurol 47:391–395. https://doi.org/10.1002/1531-8249(200003) 47:3%3c391::AID-ANA20%3e3.0.CO;2-J

- Zrzavy T, Hametner S, Wimmer I et al (2017) Loss of "homeostatic" microglia and patterns of their activation in active multiple sclerosis. Brain 140:1900–1913. https://doi.org/10.1093/brain/awx113
- Allen IV, McQuaid S, Mirakhur M, Nevin G (2001) Pathological abnormalities in the normal-appearing white matter in multiple sclerosis. Neurol Sci 22:141–144. https://doi.org/10.1007/s100720170012
- Singhal T, O'Connor K, Dubey S et al (2019) Gray matter microglial activation in relapsing vs progressive MS: a [F-18]PBR06-PET study. Neurol Neuroimmunol Neuroinflamm 6:587. https://doi.org/10.1212/ NXI.00000000000587
- Kutzelnigg A, Lucchinetti CF, Stadelmann C et al (2005) Cortical demyelination and diffuse white matter injury in multiple sclerosis. Brain 128:2705–2712. https://doi.org/10.1093/BRAIN/AWH641
- 10. Miedema A, Gerrits E, Brouwer N et al (2022) Brain macrophages acquire distinct transcriptomes in multiple sclerosis lesions and normal appearing white matter. Acta Neuropathol Commun 10:8. https://doi. org/10.1186/S40478-021-01306-3
- Bizzozero OA, DeJesus G, Callahan K, Pastuszyn A (2005) Elevated protein carbonylation in the brain white matter and gray matter of patients with multiple sclerosis. J Neurosci Res 81:687–695. https://doi. org/10.1002/inr.20587
- Sobel RA, Ahmed AS (2001) White matter extracellular matrix chondroitin sulfate/dermatan sulfate proteoglycans in multiple sclerosis. J Neuropathol Exp Neurol 60:1198–1207. https://doi.org/10.1093/JNEN/ 60.12.1198
- Vrenken H, Geurts JJG, Knol DL et al (2006) Whole-brain T1 mapping in multiple sclerosis: global changes of normal-appearing gray and white matter. Radiology 240:811–820. https://doi.org/10.1148/RADIOL.24030 50569
- Filippi M, Campi A, Dousset V et al (1995) A magnetization transfer imaging study of normal-appearing white matter in multiple sclerosis. Neurology 45:478–482. https://doi.org/10.1212/WNL.45.3.478
- Manfredonia F, Ciccarelli O, Khaleeli Z et al (2007) Normal-appearing brain t1 relaxation time predicts disability in early primary progressive multiple sclerosis. Arch Neurol 64:411–415. https://doi.org/10.1001/ ARCHNEUR.64.3.411
- Kastriti ME, Sargiannidou I, Kleopa KA, Karagogeos D (2015) Differential modulation of the juxtaparanodal complex in multiple sclerosis. Mol Cell Neurosci 67:93–103. https://doi.org/10.1016/j.mcn.2015.06.005
- Gallego-Delgado P, James R, Browne E et al (2020) Neuroinflammation in the normal-appearing white matter (NAWM) of the multiple sclerosis brain causes abnormalities at the nodes of Ranvier. PLoS Biol 18:e3001008. https://doi.org/10.1371/journal.pbio.3001008
- van den Bosch AMR, Hümmert S, Steyer A et al (2022) Ultrastructural axon-myelin unit alterations in multiple sclerosis correlate with inflammation. Ann Neurol 93:856–870. https://doi.org/10.1002/ANA.26585
- Luchicchi A, Hart B, Frigerio I et al (2021) Axon-myelin unit blistering as early event in MS normal appearing white matter. Ann Neurol 89:711–725. https://doi.org/10.1002/ana.26014
- Wheeler D, Bandaru VVR, Calabresi PA et al (2008) A defect of sphingolipid metabolism modifies the properties of normal appearing white matter in multiple sclerosis. Brain 131:3092–3102. https://doi.org/10. 1093/BRAIN/AWN190
- Poon KWC, Brideau C, Klaver R et al (2018) Lipid biochemical changes detected in normal appearing white matter of chronic multiple sclerosis by spectral coherent Raman imaging. Chem Sci 9:1586–1595. https://doi.org/10.1039/c7sc03992a
- Moscarello MA, Wood DD, Ackerley C, Boulias C (1994) Myelin in multiple sclerosis is developmentally immature. J Clin Invest 94:146–154. https://doi.org/10.1172/JCI117300
- Faigle W, Cruciani C, Wolski W et al (2019) Brain citrullination patterns and T cell reactivity of cerebrospinal fluid-derived CD4+ T cells in multiple sclerosis. Front Immunol 10:540. https://doi.org/10.3389/fimmu. 2019.00540
- Romanelli E, Merkler D, Mezydlo A et al (2016) Myelinosome formation represents an early stage of oligodendrocyte damage in multiple sclerosis and its animal model. Nat Commun 7:13275. https://doi.org/ 10.1038/ncomms13275
- 25. van Horssen J, Singh S, van der Pol S et al (2012) Clusters of activated microglia in normal-appearing white matter show signs of innate

immune activation. J Neuroinflamm 9:156. https://doi.org/10.1186/ 1742-2094-9-156

- 26. Van Der Valk P, Amor S (2009) Preactive lesions in multiple sclerosis. Curr Opin Neurol 22:207–213. https://doi.org/10.1097/WCO.0B013 E32832B4C76
- Papadopoulos K, Tozer DJ, Fisniku L et al (2010) TI-relaxation time changes over five years in relapsing-remitting multiple sclerosis. Mult Scler 16:427–433. https://doi.org/10.1177/1352458509359924
- Werring DJ, Brassat D, Droogan AG et al (2000) The pathogenesis of lesions and normal-appearing white matter changes in multiple sclerosis: a serial diffusion MRI study. Brain 123:1667–1676. https://doi.org/10.1093/ BRAIN/123.8.1667
- Elliott C, Momayyezsiahkal P, Arnold DL et al (2021) Abnormalities in normal-appearing white matter from which multiple sclerosis lesions arise. Brain Commun 3:fcab176. https://doi.org/10.1093/BRAINCOMMS/ FCAB176
- Rushton WAH (1951) A theory of the effects of fibre size in medullated nerve. J Physiol 115:101. https://doi.org/10.1113/JPHYSIOL.1951.SP004 655
- Berthold CH, Nilsson I, Rydmark M (1983) Axon diameter and myelin sheath thickness in nerve fibres of the ventral spinal root of the seventh lumbar nerve of the adult and developing cat. J Anat 136:483–508
- 32. Witte ME, Lars B, Rodenburg RJ et al (2009) Enhanced number and activity of mitochondria in multiple sclerosis lesions. J Pathol 219:193–204. https://doi.org/10.1002/path.2582
- Kiryu-Seo S, Ohno N, Kidd GJ et al (2010) Demyelination increases axonal stationary mitochondrial size and the speed of axonal mitochondrial transport. J Neurosci 30:6658–6666. https://doi.org/10.1523/JNEUROSCI. 5265-09.2010
- Zambonin JL, Zhao C, Ohno N et al (2011) Increased mitochondrial content in remyelinated axons: implications for multiple sclerosis. Brain 134:1901–1913. https://doi.org/10.1093/BRAIN/AWR110
- Périer O, Grégoire A (1965) Electron microscopic features of multiple sclerosis lesions. Brain 88:937–952. https://doi.org/10.1093/brain/88.5.937
- 36. Prineas J (1975) Pathology of the early lesion in multiple sclerosis. Hum Pathol 6:531–554. https://doi.org/10.1016/S0046-8177(75)80040-2
- 37. de Boer P, Pirozzi NM, Wolters AHG et al (2020) Large-scale electron microscopy database for human type 1 diabetes. Nat Commun 11:2475. https://doi.org/10.1038/s41467-020-16287-5
- Dittmayer C, Goebel HH, Heppner FL et al (2021) Preparation of samples for large-scale automated electron microscopy of tissue and cell ultrastructure. Microsc Microanal 27:815–827. https://doi.org/10.1017/S1431 927621011958
- Kuipers J, Giepmans BNG (2020) Neodymium as an alternative contrast for uranium in electron microscopy. Histochem Cell Biol 153:271. https:// doi.org/10.1007/S00418-020-01846-0
- Kuipers J, Kalicharan RD, Wolters AHG et al (2016) Large-scale scanning transmission electron microscopy (nanotomy) of healthy and injured zebrafish brain. J Vis Exp 2016;53635. https://doi.org/10.3791/53635
- Goebbels S, Oltrogge JH, Kemper R et al (2010) Elevated phosphatidylinositol 3,4,5-trisphosphate in glia triggers cell-autonomous membrane wrapping and myelination. J Neurosci 30:8953–8964. https://doi.org/10. 1523/JNEUROSCI.0219-10.2010
- Schindelin J, Arganda-Carreras I, Frise E et al (2012) Fiji: an open-source platform for biological-image analysis. Nat Methods 9:676–682. https:// doi.org/10.1038/NMETH.2019
- Ineichen BV, Zhu K, Carlström KE (2021) Axonal mitochondria adjust in size depending on g-ratio of surrounding myelin during homeostasis and advanced remyelination. J Neurosci Res 99:793–805. https://doi.org/10. 1002/JNR.24767
- Albert M, Antel J, Brück W, Stadelmann C (2007) Extensive cortical remyelination in patients with chronic multiple sclerosis. Brain Pathol 17:129–138. https://doi.org/10.1111/J.1750-3639.2006.00043.X
- Chomiak T, Hu B (2009) What is the optimal value of the g-ratio for myelinated fibers in the rat CNS? A theoretical approach. PLoS ONE 4:e7754. https://doi.org/10.1371/JOURNALPONE.0007754
- 46. Cercignani M, Giulietti G, Dowell NG et al (2017) Characterizing axonal myelination within the healthy population: a tract-by-tract mapping of effects of age and gender on the fiber g-ratio. Neurobiol Aging 49:109. https://doi.org/10.1016/J.NEUROBIOLAGING.2016.09.016

- Mohammadi S, Carey D, Dick F et al (2015) Whole-brain in-vivo measurements of the axonal G-ratio in a group of 37 healthy volunteers. Front Neurosci 9:441. https://doi.org/10.3389/FNINS.2015.00441/BIBTEX
- Jung W, Lee J, Shin HG et al (2018) Whole brain g-ratio mapping using myelin water imaging (MWI) and neurite orientation dispersion and density imaging (NODDI). Neuroimage 182:379–388. https://doi.org/10. 1016/J.NEUROIMAGE.2017.09.053
- Yu F, Fan Q, Tian Q et al (2019) Imaging g-ratio in multiple sclerosis using high-gradient diffusion MRI and macromolecular tissue volume. AJNR Am J Neuroradiol 40:1871–1877. https://doi.org/10.3174/AJNR.A6283
- York EN, Martin SJ, Meijboom R et al (2021) MRI-derived g-ratio and lesion severity in newly diagnosed multiple sclerosis. Brain Commun 3:fcab249. https://doi.org/10.1093/BRAINCOMMS/FCAB249
- Berg RC, Menegaux A, Amthor T et al (2022) Comparing myelin-sensitive magnetic resonance imaging measures and resulting g-ratios in healthy and multiple sclerosis brains. Neuroimage 264:119750. https://doi.org/10. 1016/J.NEUROIMAGE.2022.119750
- West KL, Kelm ND, Carson RP, Does MD (2016) A revised model for estimating g-ratio from MRI. Neuroimage 125:1155–1158. https://doi.org/10. 1016/J.NEUROIMAGE.2015.08.017
- 53. Androdias G, Reynolds R, Chanal M et al (2010) Meningeal T cells associate with diffuse axonal loss in multiple sclerosis spinal cords. Ann Neurol 68:465–476. https://doi.org/10.1002/ANA.22054
- Lovas G, Szilágyi N, Majtényi K et al (2000) Axonal changes in chronic demyelinated cervical spinal cord plaques. Brain 123:308–317. https://doi. org/10.1093/BRAIN/123.2.308
- Nikić I, Merkler D, Sorbara C et al (2011) A reversible form of axon damage in experimental autoimmune encephalomyelitis and multiple sclerosis. Nat Med 17:495–499. https://doi.org/10.1038/NM.2324
- Steyer AM, Buscham TJ, Lorenz C et al (2022) Focused ion beam-scanning electron microscopy links pathological myelin outfoldings to axonal changes in mice lacking PIp1 or Mag. Glia 71:509–523. https://doi.org/10. 1002/GLIA.24290
- 57. Gibson EM, Purger D, Mount CW et al (2014) Neuronal activity promotes oligodendrogenesis and adaptive myelination in the mammalian brain. Science 344:1252304. https://doi.org/10.1126/science.1252304
- Meschkat M, Steyer AM, Weil MT et al (2022) White matter integrity in mice requires continuous myelin synthesis at the inner tongue. Nat Commun 13:1163. https://doi.org/10.1038/S41467-022-28720-Y
- Recks MS, Stormanns ER, Bader J et al (2013) Early axonal damage and progressive myelin pathology define the kinetics of CNS histopathology in a mouse model of multiple sclerosis. Clin Immunol 149:32–45. https:// doi.org/10.1016/J.CLIM.2013.06.004
- Kolaric KV, Thomson G, Edgar JM, Brown AM (2013) Focal axonal swellings and associated ultrastructural changes attenuate conduction velocity in central nervous system axons: a computer modeling study. Physiol Rep 1:e00059. https://doi.org/10.1002/PHY2.59
- Paus T, Toro R (2009) Could sex differences in white matter be explained by g ratio? Front Neuroanat 3:14. https://doi.org/10.3389/NEURO.05.014. 2009
- Bouhrara M, Kim RW, Khattar N et al (2021) Age-related estimates of aggregate g-ratio of white matter structures assessed using quantitative magnetic resonance neuroimaging. Hum Brain Mapp 42:2362–2373. https://doi.org/10.1002/HBM.25372
- Fan Q, Tian Q, Ohringer NA et al (2019) Age-related alterations in axonal microstructure in the corpus callosum measured by high-gradient diffusion MRI. Neuroimage 191:325. https://doi.org/10.1016/J.NEUROIMAGE. 2019.02.036
- 64. Stahon KE, Bastian C, Griffith S et al (2016) Age-related changes in axonal and mitochondrial ultrastructure and function in white matter. J Neurosci 36:9990–10001. https://doi.org/10.1523/JNEUROSCI.1316-16.2016

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